

Utilization of Single Whole Body Vibration Training Unit in Rehabilitation of Elderly Patients with Neurological Disorders

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Abstract-Whole body vibration (WBV) techniques are increasingly applied in rehabilitation processes to improve patients' functional mobility. Therapeutic usage of WBV reported enhanced muscular strength, power or even bone density. Therefore, the purpose of our study was to investigate immediate response of single WBV training unit on mobility of elderly patients with neurological disorders. Nineteen patients $(66.74 \pm 3.65 \text{ years}, 6 \text{ males and } 13 \text{ females})$ were assessed before WBV (10 min, 30 Hz, vertical 2 mm) and then 1 min afterwards. Individual changes in gait kinematics indicated positive effects of WBV, while kinematics of the gait was more symmetric considering right and left side. Individually, depending on the disease's severity, these changes were more or less significant. The improvements in gait kinematics convinced us that WBV can be carefully used in patients' therapy and it may be used together with individually planed rehabilitation processes to bring more satisfying results.

I. INTRODUCTION

Ageing of the population brings growing demands on social and health care systems due to the increased risks of various chronic diseases in older individuals. Health related quality of human life and loss of independence can be also affected by natural weakening of human body and its functional systems. This leads to more frequent falls and consecutive health and mobility problems [1-3].

Here, the disorders like sensory loss, vestibular dysfunction, impaired vision, muscular weakness, bone rarefaction or gait disorders are multi-factorial disorders that contribute to vulnerability and frailty of elderly persons. Moreover, elderly falls are usually reasons for additional medical interventions. Motor impairment syndromes are also associated with neurological disorders [4]. This group of clinically heterogeneous diseases causes severe problems in coordination, gait, balance, voluntary muscle control, power and strength [5, 6].

Strategies to prevent negative consequences of functional mobility diseases have to be widely discussed, assessed and applied in health care of elderly patients. Such strategies include also rehabilitation techniques and physical exercises. Here, due to the published results the WBV can be considered as reliable and effective tool in rehabilitation and sport medicine [7, 8].

Continuing in our previous pilot study [9] we hypothesize that the WBV may stimulate muscle activation in elderly patient with neurological disorders and that application of WBV will result in improvement of quality of their gait. Therefore, the purpose of this study was to investigate whether the single WBV session has any positive effects on gait kinematics.

II. WHOLE BODY VIBRATION

Whole body vibration (WBV) has been extensively studied for its dangerous effects on humans, especially when exposed as occupational vibration at high amplitudes and specific frequencies [10-12]. However, WBV is also the concept that was already applied in many studies to confirm benefits for astronauts, athletes, wellness of healthy population, but also patients with various diseases [13-15].

Recent clinical works suggest that low amplitude and low frequency of mechanical stimulation of the human body is a safe and effective way to exercise musculoskeletal structures. The studies realized during past decade indicate that WBV may increase muscle strength, neuromuscular function, bone mass and mineral density [16-19], can be useful in improving physical capacity, cardiorespiratory functions, hormonal production, proprioception, and balance [20-22].

Despite of WBV positive effects presented in almost all related research studies, the authors interpret their results with caution. Also, the underlying mechanisms by which WBV enhance neuromuscular performance vary between studies and are still unclear. Inconsistency in presented results is caused by various training protocols and heterogeneity in study designs. However, several mechanisms should be considered as crucial. Vibration stimulates skeletal muscle by activating a stretch reflex analogous to the tonic vibration reflex. Thus the activated muscle spindle activity causes involuntary reflexive muscle contraction in an attempt to control the vibration imposed muscle length change. WBV also evoke changes in postural control strategy where the vibration stimulus generates postural instability and the body activates particular muscles to maintain body balance. Another mechanism is generated

when oscillations induce a muscle tuning response in an attempt to minimize the propagation of the vibrations throughout the body. Then, the muscles might activate to prevent further transmission of the vibration stimulus through the body.

There are various vibrating platforms available as commercial products used by many wellness centers and rehabilitation clinics. The main differences are in the type of vibration stimulation, frequency range, and amplitude of vibration [23, 24]. Most of the vibrating platforms vibrate sinusoidally. The subjects stand on the platform which oscillates only vertically or side alternating. Other types of vibrating devices uses two separate platforms to produce vibrations for each foot independently. While commercial usage promotes WBV as attractive and effective alternative to resistance training, the therapeutic applications should carefully consider duration of WBV exposure, main vibration characteristics as well as their effects on neuromuscular system respecting patients' physical capabilities. The rest periods between vibration trainings may also play a significant role in final WBV effects. The effect of vibration may be also tested using various modeling techniques [25].

III. MATERIAL AND METHODS

A. Patients

A group of nineteen elderly patients (age 66.74 ± 3.65 years, 6 males and 13 females) with various neurological disorders were included in the study. The inclusion criteria were ambulatory patients that are able to walk independently, had no cardiovascular disease or epilepsy, and had no prior experience in WBV training. All the patients were informed about the WBV training, about the tests to be realized and also about possible risks and benefits of the research. Prior to participation they gave written informed consent approved together with the study design by the University Hospital Ethics Committee.

All participants attended a familiarization session before the study and before the tests were performed. No other physical treatment or intervention was realized at least 24 hour before WBV training session. The anthropometric measures were also taken and registered in patients' experimental protocols. As for the aim of the study, the anthropometric characteristics of lower extremities were preferred, including thigh length (right: 44.89 ± 2.26 cm, left: 44.42 ± 2.14 cm), calf length (right: 41.89 ± 3.80 cm, left: 41.58 ± 3.91 cm) and foot length (right: 25.74 ± 2.82 cm, left: 25.89 ± 2.55 cm).

B. Experiment

The experimental protocol was designed to discover potential immediate response of a single WBV training unit to the quality of gait kinematics in elderly patients. Training sessions were supervised by rehabilitation specialist and measurements as well as WBV sessions were conducted in the same thermally neutral room intended for physical training. All subjects did not engage in any therapeutic or rehabilitation procedures before testing.

The training session started with physical examination and short warming-up walk. Then, the patient's gait was captured and analyzed before WBV exposure. Participants were asked to walk at their natural waking speed along the 6 m long path. After reaching the end point of the path, they were asked to turn back (180°), i.e. to change the direction of gait, and to walk back to the starting point. Then, they turned back again and walked to the end point of the path, where the last turn back was realized and the patients finished walking in starting point of the path. In that sense, the subjects passed the length of walking path four times. WBV session followed one minute after this control gait was captured and analyzed. Here, each participant stood in static position on the vibration platform (VibroGym inSPORTline) with no shoes and socks and holding on the device handle. Erected posture with slightly bended knees was required during vibration test. The patients were asked to stop the training in the case of any pain responses to vibration. Duration of one WBV training unit was set to 10 min. Sinusoidal vertical vibration frequency was set to 30 Hz with amplitude of 2 mm. 1 min rest interval followed after this WBV exposure. Then, the patients walked again and the kinematics of their gait was captured and analyzed in the same way as it was before WBV session. Finally, the kinematics obtained before and after WBV training unit was compared to evaluate its effects on patients' gait.

C. Parameters

Gait assessment was performed using our marker-free motion analysis system MAFRAN [26]. The system is based on motion tracking method in video sequence with no passive or active markers attached to the patients' bodies tries to minimize disadvantages of currently available marker-free systems, to bring new of motion analysis and to offer clinicians cheaper, but not worse alternative preserving all advantages of motion analysis.

Here, the patient's gait is captured in sagittal plane using common commercial video camera. Then, the raw record is used in the system to automatically reconstruct motion trajectories of human body anatomical landmarks, i.e. the trajectories of all lower extremity joints and adjacent segments. These trajectories are consequently used to calculate other kinematical parameters for detailed description of patient's gait. Here analyzed parameters include positions, velocities and accelerations of individual joints, hip flexion/extension, knee flexion/extension, and ankle plantar/dorsal flexion angles, gait cycle length, gait cycle time, gait cycle velocity, cadence (cycles per minute), stance phase and swing phase of the gait cycle.

D. Statistics

All acquired kinematical parameters were analyzed individually within the patient and then within the group of here included patients as well. The kinematical characteristics of the patients were evaluated as differences between right and left side. The hypothesis was based on assumption that these differences should be smaller after WBV training comparing values obtained before WBV training. Otherwise, the WBV will probably have no immediate benefits for gait kinematics. Statistical methods included descriptive statistics and Student's paired t-test and were used to ascertain specific and significant differences. The significance level was set to P < 0.05.

IV. RESULTS

WBV session was well accepted by all elderly patients included in this continuing study. No one felt any pain or expressed any problems during WBV exposure. A first analysis was performed with anatomical joint angles of lower extremities in sagittal plane. Individually, no of the patients had the same curves of all tree joints comparing before and after WBV values. At least one joint's trajectory was changed either in positive or negative direction. An example of anatomical joint angles changes in 65 years old male patient with right hemiparesis is shown on following figures.

Figure 1 shows hip flexion/extension angle before and after single WBV training unit. A paired t-test determined that the mean decrease of differences (M=0.47, SD=4,29, N=51) was not significantly greater than zero, t(50)=0.78, two-tail p=0.441 (95% CL=1.208), providing evidence that the WBV was not effective in reduction of differences between right and left hip flexion/extension angle.

Figure 2 shows knee flexion/extension angle before and after single WBV training unit. Knee flexion/extension angle of the same patient showed that the mean differences between right and left side before and after WBV were decreased, but the mean decrease of differences (M=0.54, SD=8,207, N=51) was not significantly greater than zero, t(50)=0,47, two-tail p=0.643 (95% CL=2.308), providing evidence that the WBV was not effective in reduction of differences between right and left knee flexion/extension angle in this patient.

Figure 3 shows ankle plantar/dorsal flexion angle before and after single WBV training unit. The mean decrease of the right and the left side differences in ankle plantar/dorsal flexion angle of the same 65 years old male patient (M=3.79, SD=4,089, N=51) was significantly greater than zero, t(50)=6.63, two-tail p=0.000 (95% CL=1.150) provided evidence that the WBV was effective in reduction of differences between right and left ankle plantar/dorsal flexion angle.

Anatomical joint angles were analyzed in all participants of this study in the same way. The summary of right and lefts side differences in anatomical joint angles in elderly patients showed that the most significant changes were registered in the ankle plantar/dorsal flexion angle (89.47%), followed by hip flexion/extension angle (73.68%) and knee (57.89%). flexion/extension angle However, these significant changes include both the positive and the negative changes. The only significant positive changes were chiefly in hip flexion/extension angle (63.16%) followed by the knee flexion/extension angle (47.37%) and ankle plantar/dorsal flexion angle (47.37%).

Individually, there were thirteen patients (68.42%) who had at least two significant positive changes of these kinematical parameters or they had no significant negative



Fig. 1 Hip flexion/extension angle in 65 years old male patient with right hemiparesis before and after WBV exposure (solid line – right leg, dashed line – left leg).



Fig. 2 Knee flexion/extension angle in 65 years old male patient with right hemiparesis before and after WBV exposure (solid line – right leg, dashed line – left leg).



Fig. 3 Ankle plantar/dorsal flexion angle in 65 years old male patient with right hemiparesis before and after WBV exposure (solid line – right leg, dashed line – left leg).

changes (subjects 1, 2, 3, 5, 8, 9, 10, 13, 14, 15, 17, 18 and 19). Two patients (10.53%) had no beneficial improvements resulting from applied WBV exposure (subjects 6 and 12) and four patients (21.05%) of the elderly patient subgroup registered worsening because of no significantly positive or only significantly negative changes (subjects 4, 7, 11 and 16).

The second analysis was performed in spatial-temporal parameters. Here, the symmetry of all characteristics was examined and summarized. The mean differences between right and left sides and standard deviations of these parameters are listed in the table 1.

No of here analyzed parameters had significantly neither positive nor negative changes. Nevertheless, some of the parameters had positive and another negative tendency. The positive trends were shown in decreasing differences between right and left side in gait cycle length (1.470 \pm 6.417) and velocity (0.016 \pm 0.056). On the other side small increase was registered in cadence (-0.064 \pm 1.507) and gait cycle stance (-0.885 \pm 4.951 and swing (-0.907 \pm 4.932) phase. Gait cycle time remained almost unchanged (0.002 \pm 0.043).

V. CONCLUSION

In this study, the effect of single WBV training unit was tested in elderly patients with neurological disorders including multiple sclerosis, Parkinson disease, cerebral palsy and radiculoneuritis. The significant improvement was confirmed mainly in anatomical joint angles rather than in spatial-temporal parameters. As we expected, the single whole body vibration training unit had only short-time effect as six of the beneficial patients were analyzed one week after the experiment and their kinematics was similar to the pre- exposure status. Utilization of WBV training in patients with neurological disorders may result in benefits for kinematics of human motion, but its significance and mechanism still remains unclear and undiscovered.

The results of this pilot study provided invaluable data for rehabilitation specialists as well as for development of further research programs in physiotherapy. Based on the results we obtained, it was also confirmed that an individual WBV training and supervised functional treatment should be specified for particular patient. Further research should be realized to clarify WBV specific benefits. The various training approaches including standing in different static positions, sitting on chair with legs on vibrating platform or performing exercises on the platform during therapy sessions should be investigated as well.

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Parameter	Pre WBV	Post WBV	Delta pre/post
GC length (cm)	5.751 ± 4.170	4.281 ± 4.708	1.470 ± 6.417
GC time (s)	0.086 ± 0.075	0.084 ± 0.077	0.002 ± 0.043
GC velocity (m/s)	0.067 ± 0.038	0.051 ± 0.048	0.016 ± 0.056
Cadence (GC/min)	2.014 ± 1.284	2.078 ± 1.286	-0.064 ± 1.507
Stance phase (%)	3.556 ± 2.944	4.441 ± 4.984	-0.885 ± 4.951
Swing phase (%)	3.562 ± 2.942	4.469 ± 4.963	-0.907 ± 4.932

TABLE I. Spatial-temporal characteristics of patients' gait obtained before (Pre) and after (Post) WBV exposure (N=19).

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